



## Heat Transfer In A Two-Layered Blood Flow Model In A Narrow Tube In Presence Of Magnetic Field

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### abstract

Blood flow in a narrow tube is described using the two-layered model in presence of an external uniform magnetic field. The model consists of a core region, enriched with various types of blood cells and a cell-free peripheral plasma layer. Also the constant heat flux convective heat transfer to fully developed blood flow is studied. The velocity and temperature profiles are determined. The expressions for friction-factor-Reynolds number product and Nusselt number are found and their natures are shown graphically.

**Keywords:**two-layered-model, convective heat transfer, friction-factor-Reynolds number, Nusselt number.

### I. INTRODUCTION

The regulation of body temperature is mainly done by the circulatory system. Body heat produced by the skeletal muscle is in general removed by the convection heat transfer of blood [1]. It is also observed that the smaller blood vessels are more actively engaged in the heat exchange with the surroundings. So, the thermally important blood vessels are of very small diameter and are in the range of 50–500  $\mu\text{m}$  [2,3]. Researchers have made number of investigations regarding the heat transfer between the small blood vessels and their surrounding tissues [4,5,6]. Wang [7] studied the fully developed heat transfer in a narrow vessel using the two-fluid model. Convective heat transfer of blood is of much importance in the use of various clinical aspects such as local hyperthermia, cryosurgery for tumor treatment etc.

To determine the convective heat transfer from a blood vessel, we have to first find out the velocity profile. In larger vessels the nature of blood is almost homogeneous and we may readily compute the heat transfer using parabolic (i.e., Poiseuille) velocity distribution [8]. But for flow in narrow vessels, the blood cells tend to migrate along the centre of the vessel which give rise to a core region in which the concentration of blood cells is high, and a slower moving peripheral plasma region which is almost cell free [9,10]. So the flow of blood in a narrow vessel may be explained by a two-layered model [11,12,13]. A good number of models have been developed regarding this phenomenon [14,15]. Pries et al. derived empirical relationships of the relative apparent viscosity and mean tube hematocrit from in vitro [16,17] and in vivo [18].

In the present analysis we study the effect of an external magnetic field on the convective heat transfer of blood in a narrow vessel. The analytical expressions of velocity for blood and temperature in core

region as well as in peripheral plasma region are determined. Also the expressions for friction-factor-Reynolds number and Nusselt number are obtained. The effect of magnetic field and thickness of core region on them are shown through graphs.

## II. MATHEMATICAL FORMULATIONS AND SOLUTIONS

We consider a two-fluid model for blood flow within a narrow cylindrical tube of radius R and length L. The core region is assumed to be enriched with various kinds of blood cells with radius  $r_c$  and effective viscosity  $\mu_c$ . The cell free plasma layer has the effective viscosity  $\mu_0$ . Thus this model consists of two immiscible fluids (Fig. 1).

Let us consider r and z be the radial and axial directions in the tube,  $u_c$  and  $u_0$  be the velocity of blood in the core region and peripheral plasma region respectively along the axial direction.

The basic equations may be written in the form

$$-\frac{\partial p}{\partial z} + \frac{\mu_c}{r} \frac{\partial}{\partial r} \left( r \frac{\partial u_c}{\partial r} \right) - \sigma B_0^2 u_c = 0 \quad ; \quad 0 \leq r \leq r_c \quad (2.1)$$

for the core region and

$$-\frac{\partial p}{\partial z} + \frac{\mu_0}{r} \frac{\partial}{\partial r} \left( r \frac{\partial u_0}{\partial r} \right) = 0 \quad ; \quad r_c < r \leq R \quad (2.2)$$

for peripheral plasma region, where  $\frac{\partial p}{\partial z}$  is the pressure gradient,  $\sigma$  is the electrical conductivity of the medium and  $B_0$  is the transverse component of the magnetic field. As the peripheral plasma layer is considered cell free, the effect of  $B_0$  is negligible in this region.

The boundary conditions for velocity are given as

(a)  $u_c$  is bounded on the axis and because of symmetry, the velocity gradient vanishes along the axis of the tube:

$$\frac{\partial u_c}{\partial r} = 0 \quad \text{at } r = 0. \quad (2.3)$$

(b) There is no slip on the wall:

$$u_0 = 0 \quad \text{at } r = R. \quad (2.4)$$

(c) The velocity and shear stress are continuous at the interface of the two layers:

$$(i) \quad u_c|_{r=r_c} = u_0|_{r=r_c}, \quad (2.5)$$

$$(ii) \quad \mu_c \frac{\partial u_c}{\partial r} \Big|_{r=r_c} = \mu_0 \frac{\partial u_0}{\partial r} \Big|_{r=r_c}. \quad (2.6)$$

Taking  $\xi = \frac{r}{R}$ ,  $\lambda = \frac{r_c}{R}$ ,  $P = -\frac{1}{R} \frac{\partial p}{\partial z}$  and using the boundary conditions (2.3)-(2.6) we obtain the solutions of (2.1) and (2.2) as

$$\left. \begin{aligned} u_c &= \frac{J_0(a\xi)}{J_0(a\lambda)} \left\{ \frac{PR^2}{4\mu_0} (1 - \lambda^2) - \frac{P}{\sigma B_0^2} \right\} + \frac{P}{\sigma B_0^2}; 0 \leq \xi \leq \lambda \\ u_0 &= \frac{PR^2}{4\mu_0} (1 - \xi^2); \lambda \leq \xi \leq 1 \end{aligned} \right\} \quad (2.7)$$

where  $a = iB_0R\sqrt{\frac{\sigma}{\mu_c}}$ .

Let V be the mean velocity, so that  $\pi V$  gives the total flow. Therefore

$$\begin{aligned} V &= 2 \left\{ \int_0^{r_c} u_c r dr + \int_{r_c}^R u_0 r dr \right\} \\ &= \frac{2R^2\lambda}{\alpha} \frac{J_1(a\lambda)}{J_0(a\lambda)} \left\{ \frac{PR^2}{4\mu_0} (1 - \lambda^2) - \frac{P}{\sigma B_0^2} \right\} + \frac{PR^2\lambda^2}{\sigma B_0^2} + \frac{PR^2}{8\mu_0} (1 - \lambda^2)^2. \end{aligned} \quad (2.8)$$

Now we consider  $T(r,z)$  as the temperature and  $q$  as the constant heat flux applied on the wall. Assuming  $T_c$  as the temperature on the core region and  $T_0$  as the temperature on peripheral plasma layer we may construct the forced convection equations as

$$P_c u_c \frac{\partial T_c}{\partial z} = \frac{1}{r} \frac{\partial}{\partial r} \left( r \frac{\partial T_c}{\partial r} \right), \tag{2.9}$$

for the core region and

$$\beta P_c u_0 \frac{\partial T_0}{\partial z} = \frac{1}{r} \frac{\partial}{\partial r} \left( r \frac{\partial T_0}{\partial r} \right), \tag{2.10}$$

for the peripheral plasma region, where  $P_c$  is the Peclet number and  $\beta \left( = \frac{\kappa_c}{\kappa_0} \right)$  is the ratio of the thermal diffusivities.

Let us introduce two new parameters;  $\gamma \left( = \frac{k_c}{k_0} \right)$ , the ratio of conductivities and  $T_m$ , the mean temperature given by

$$T_m(z) = \frac{2}{V} \left\{ \int_0^{r_c} u_c T_c r dr + \int_{r_c}^R u_0 T_0 r dr \right\}. \tag{2.11}$$

For constant flow problem, all the temperatures must have same constant gradient (say  $A$ ) in the axial direction. Thus we may write

$$\frac{\partial T_c}{\partial z} = \frac{\partial T_0}{\partial z} = \frac{\partial T_m}{\partial z} = A. \tag{2.12}$$

The boundary conditions for temperature are given as :

- (a)  $T_c$  is bounded on the axis,
- (b) the heat flux on the wall is

$$\frac{\partial T_0(R, z)}{\partial r} = \gamma, \tag{2.13}$$

- (c) the temperature and fluxes match on the interface, i.e.,

$$(i) \quad T_c(r_c, z) = T_0(r_c, z), \tag{2.14}$$

$$(ii) \quad \gamma \frac{\partial T_c(r_c, z)}{\partial r} = \frac{\partial T_0(r_c, z)}{\partial r}, \tag{2.15}$$

- (d)

$$T_m(0) = 0. \tag{2.16}$$

Applying the aforementioned boundary conditions and the same non-dimensionalisation scheme used for velocity profile, we obtain the solutions of (2.9) and (2.10) as

$$T_c = Az - \frac{P_c R^2 A J_0(a\xi)}{a^2 J_0(a\lambda)} \left\{ \frac{PR^2}{4\mu_0} (1 - \lambda^2) - \frac{P}{\sigma B_0^2} \right\} + \frac{PP_c R^2 A}{4\sigma B_0^2} \xi^2 + C_1, \tag{2.17}$$

$$T_0 = Az + \frac{\beta PP_c R^4 A}{4\mu_0} \left\{ \frac{\xi^2}{4} - \frac{\xi^4}{16} + C_2 \ln \xi + C_3 \right\}. \tag{2.18}$$

The constants  $A$ ,  $C_1$ ,  $C_2$  and  $C_3$  can be determined from the boundary conditions (2.13)-(2.16) and are given in the appendix.

The friction-factor-Reynolds number product  $fRe$  is defined as [7]  
 $fRe = \frac{8}{V}$

$$= \frac{8}{\frac{2R^2\lambda}{\alpha} \frac{J_1(a\lambda)}{J_0(a\lambda)} \left\{ \frac{PR^2}{4\mu_0} (1 - \lambda^2) - \frac{P}{\sigma B_0^2} \right\} + \frac{PR^2\lambda^2}{\sigma B_0^2} + \frac{PR^4}{8\mu_0} (1 - \lambda^2)^2}. \tag{2.19}$$

We also obtain the gauge for the heat transfer, known as Nusselt number, and its value is computed numerically using the formula

$$Nu = \frac{2}{T_0(R, z) - T_m(z)}. \tag{2.20}$$

Numerically it can be shown that all the above analytical results agree with the previous results [13,7] when  $B_0 \rightarrow 0$ .

### III. NUMERICAL RESULTS AND DISCUSSIONS

The velocity in the core region and in the peripheral plasma layer are obtained in equation (2.7). The values of these velocity profiles are computed and depicted through the figs. 2 and 3. The effect of the transverse component of the magnetic field  $B_0$  is also shown in that figures. In those figures we observe that the velocity decreases with the increase in the value of  $B_0$ .

In fig. 4, the nature of velocity profile is shown for different values of  $\lambda$  taking  $B_0=0.02$ . Here we observe that the velocity profile decreases with the increase in the values of  $\lambda$ .

In fig. 5, the behavior of temperature profile is shown for  $\lambda= 0.7$ . From this figure it is clear that the transfer of heat occurs mainly in the peripheral plasma layer. In the core region as the value of  $r$  increases the value of temperature profile increases negligibly; but in the peripheral plasma layer the value of temperature profile increases much more rapidly with the increase in the values of  $r$ . Also the heat transfer decreases as the magnetic field  $B_0$  increases.

From equation (2.19) the values of friction-factor-Reynolds number  $fRe$  are computed and the effect of the magnetic field  $B_0$  on  $fRe$  is shown through the fig. 6. Here we observe that the value of  $fRe$  increases as the value of  $B_0$  increases.

The values of Nusselt number  $Nu$  are calculated using equation (2.20) and the variation of  $Nu$  against  $\lambda$  is shown on fig. 7. Here we observe that the Nusselt number is effected largely by the magnetic field  $B_0$ . It increases with the increase in the values of  $B_0$ . For  $\lambda=0$ ,  $Nu$  becomes 0.436 and whenever  $\lambda$  tends to one,  $Nu$  tends to zero for any value of  $B_0$ .

### IV. CONCLUSIONS

In biological systems, the regulation of body temperature is of great importance and is mainly maintained by the blood vessels. From our present discussions the amount and nature of heat transfer through the blood vessels can be calculated. Using an external magnetic field we can regulate the heat transfer.

### V. APPENDIX

From the boundary condition (2.13) we obtain the value of  $A$  as

$$A = \frac{R\gamma}{\frac{P_c R^2 \lambda J_1(a\lambda)}{a J_0(a\lambda)} \left\{ \frac{PR^2}{4\mu_0} (1 - \lambda^2) - \frac{P}{\sigma B_0^2} \right\} + \frac{PP_c R^2 \gamma \lambda^2}{2\sigma B_0^2} - \frac{\beta PP_c R^4}{4\mu_0} \left( \frac{\lambda^2}{2} - \frac{\lambda^4}{4} \right) + \frac{\beta PP_c R^4}{16\mu_0}}$$

and from the boundary condition (2.15) we obtain the value of  $C_2$  as

$$C_2 = \frac{4\mu_0}{\beta R^2} \left[ \frac{\gamma \lambda J_1(a\lambda)}{a J_0(a\lambda)} \left\{ \frac{R^2}{4\mu_0} (1 - \lambda^2) - \frac{1}{\sigma B_0^2} \right\} + \frac{\gamma \lambda^2}{2\sigma B_0^2} - \frac{\beta R^2}{4\mu_0} \left( \frac{\lambda^2}{2} - \frac{\lambda^4}{4} \right) \right].$$

From the boundary conditions (2.14) and (2.16) we obtain two relations connecting  $C_1$  and  $C_3$  namely

$$C_1 = PP_cR^2A \left[ \frac{\beta R^2}{4\mu_0} C_3 + \left\{ \frac{\beta R^2}{4\mu_0} \left( \frac{\lambda^2}{4} - \frac{\lambda^4}{16} + C_2 \ln \lambda \right) + \frac{R^2}{4\mu_0 a^2} (1 - \lambda^2) - \frac{1}{\sigma B_0^2 a^2} - \frac{\lambda^2}{4\sigma B_0^2} \right\} \right]$$

and

$$\begin{aligned} \frac{2R^2}{V} \left[ \frac{Az\lambda J_1(a\lambda)}{aJ_0(a\lambda)} \left\{ \frac{PR^2}{4\mu_0} (1 - \lambda^2) - \frac{P}{\sigma B_0^2} \right\} + \frac{PAz\lambda^2}{2\sigma B_0^2} - \frac{P_cR^2A\lambda^2}{2a^2J_0^2(a\lambda)} \{J_0^2(a\lambda) \right. \\ \left. + J_1^2(a\lambda)\} - \frac{PP_cR^2A\lambda J_1(a\lambda)}{\sigma B_0^2 a^3 J_0(a\lambda)} \left\{ \frac{PR^2}{4\mu_0} (1 - \lambda^2) - \frac{P}{\sigma B_0^2} \right\} \right. \\ \left. + \frac{PP_cR^2A}{4\sigma B_0^2 J_0(a\lambda)} \left\{ \frac{PR^2}{4\mu_0} (1 - \lambda^2) - \frac{P}{\sigma B_0^2} \right\} \int_0^\lambda \xi^2 J_0(a\xi) d\xi \right. \\ \left. + \frac{P^2P_cR^2A\lambda^3}{12\sigma^2 B_0^4} + \frac{C_1\lambda J_1(a\lambda)}{aJ_0(a\lambda)} \left\{ \frac{PR^2}{4\mu_0} (1 - \lambda^2) - \frac{P}{\sigma B_0^2} \right\} + \frac{PC_1\lambda^2}{2\sigma B_0^2} \right] \\ + \frac{2R^2}{V} \left[ \frac{PR^2Az}{4\mu_0} \left( \frac{1}{4} - \frac{\lambda^2}{2} + \frac{\lambda^4}{4} \right) + \frac{\beta P^2P_cR^6A}{16\mu_0^2} \left\{ \frac{C_3}{2} (1 - \lambda^2) \right. \right. \\ \left. \left. + \left( \frac{1}{16} - \frac{C_3}{4} \right) \left( 1 - \frac{\lambda^4}{4} \right) - \frac{5}{96} (1 - \lambda^6) + \frac{1}{128} (1 - \lambda^8) \right. \right. \\ \left. \left. + C_2 \left( -\frac{1}{4} - \frac{\lambda^2}{2} \ln \lambda + \frac{\lambda^2}{4} \right) - C_2 \left( -\frac{1}{16} - \frac{\lambda^4}{4} \ln \lambda + \frac{\lambda^4}{16} \right) \right\} \right] = 0. \end{aligned}$$

Solving these two equations numerically we get the values for  $C_1$  and  $C_3$ .

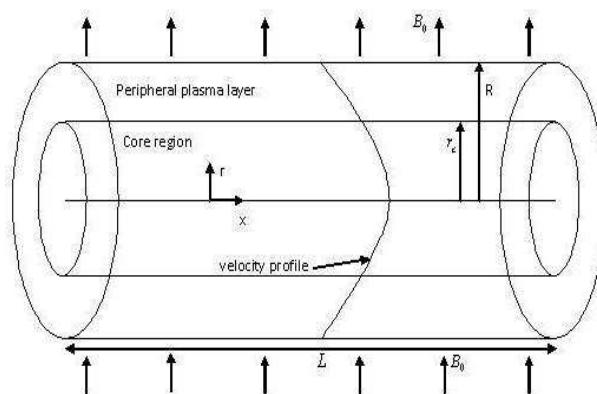


Fig. 1 : Schematic diagram of the model

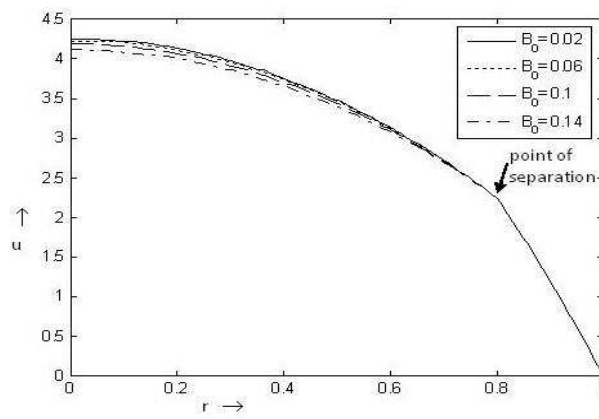


Fig. 2: Velocity profile taking  $\lambda = 0.8$ .

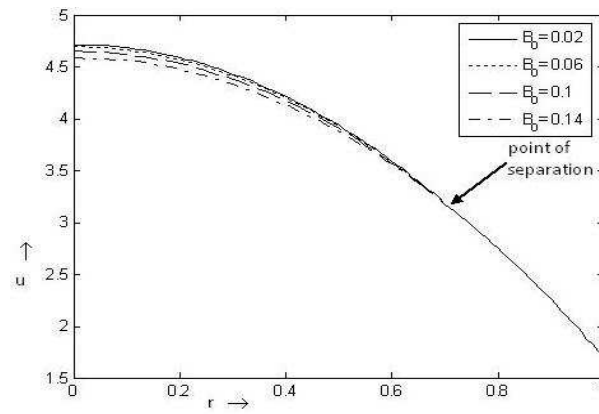


Fig. 3: Velocity profile taking  $\lambda = 0.7$ .

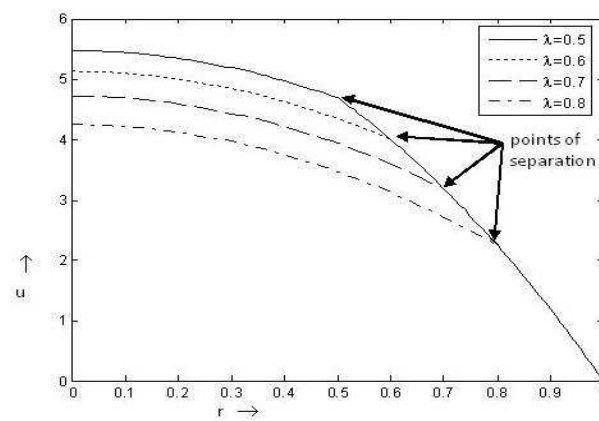


Fig. 4: Velocity profile taking  $\beta_0 = 0.02$ .

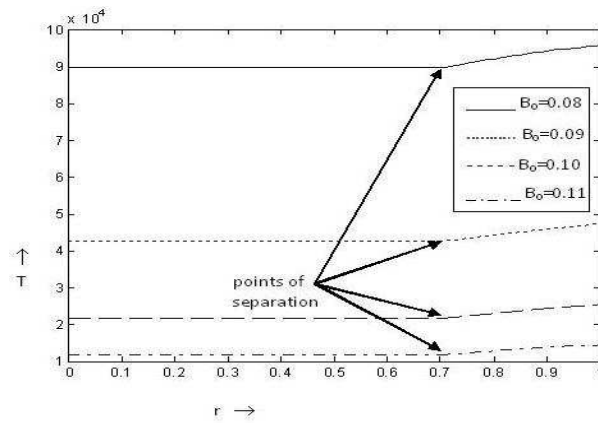


Fig. 5 : Temperature profile taking  $\lambda = 0.7$ .

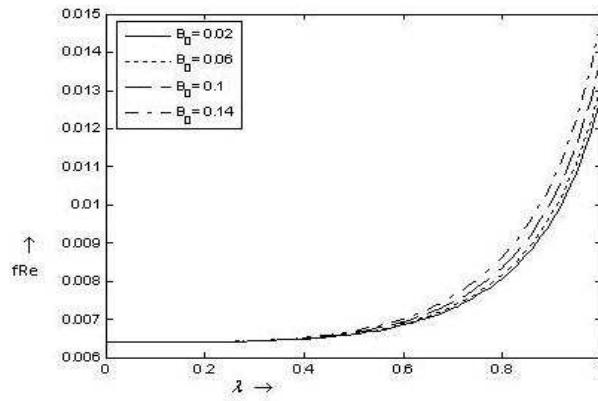


Fig. 6 :  $fRe$  as a function of  $\lambda$ .

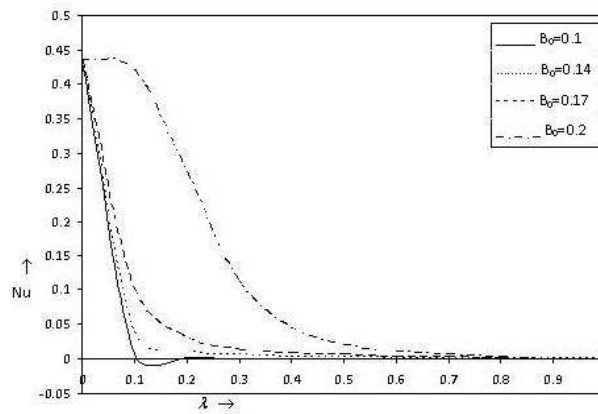


Fig. 7 : Nusselt number as a function of  $\lambda$ .

## REFERENCES

1. Schottelius, B.A. and Schotteliys, D.D. : Textbook of Physiology, 18th ed., Mosby St. Louis, 1978.
2. Chen, M.M. and Holmes, K.R. : Microvascular Contributions in Tissue Heat Transfer, Annals of the New York Academy of Sciences, 1980, **335**:137-151.
3. Chato, J.C. : Heat Transfer to Blood Vessels, Journal of Biomedical Engineering, 1980, **102**:110-118.
4. Arkin, H., Xu, L.X. and Holmes, K.R. : Recent Developments in Modeling Heat Transfer in Blood Perfused Tissues, IEEE, Transactions on Biomedical Engineering, 1994, **41**:97-107.
5. Crezee, J., Mooibroek, J., Lagendijk, J.J.W. and Van Leeuwen, G.M.J. : The Theoretical and Experimental Evaluation of the Heat Balance in Perfused Tissue, Physics in Medicine and Biology, 1994, **39**:813-832.
6. Diller, K.R. and Ryan, T.P. : Heat Transfer in Living Systems : Current Opportunities, ASME Journal of Heat Transfer, 1998, **120**:810-829.
7. Wang, C.Y. : Heat Transfer to Blood Flow in a Small Tube, Journal of Biomechanical Engineering, 2008, **130**:024501-1-024501-3.
8. Shah, R.K. and London, A.L. : Laminar Flow Forced Heat Convection in Ducts, Academic, New York, 1978.
9. Pries, A.R., Secomb, T.W. and Gaehtgens, P. : Biophysical Aspects of Blood Flow in the Microvasculature, Cardiovascular Research, 1996, **32**:654-667.
10. Mchedlishvili, G. and Maeda, N. : Blood Flow Structure Related to Red Cell Flow : A Determinant of Blood Fluidity in Narrow Microvessels, The Japanese Journal of Physiology, 2001, **51**:19-30.
11. Fahreaus, R. and Lindqvist, T. : The Viscosity of Blood in Narrow Capillary Tubes, American Journal of Physiology, 1931, **96**:562-568.
12. Hayes, R.H. : Physical Basis of the Dependence of Blood Viscosity on tube Radius, American Journal of Physiology, 1960, **198**:1193-1200.
13. Sharan, M. and Popel, A.S. : A Two-Phase Model for Flow of Blood in Narrow Tubes With Increased Effective Viscosity Near the Wall, Biorheology, 2001, **38**:415-428.
14. Whitmore, R.L. : A Theory of Blood Flow in Small Vessels, Journal of Applied Physiology, 1967, **22**:767-771.
15. Chein, S., Usami, S., Skalak, R. : Blood Flow in Small Tubes, Handbook of Physiology, Section2 : The Cardiovascular System IV, Part I : Microcirculation, Reknin, E.M. and Michel, C.C., eds., American Physiological Society, Bethesda, MD, 1984, 217-249.
16. Pries, A.R., Secomb, T.W., Gaehtgens, P. and Gross, J.F. : Blood Flow in Microvascular Networks : Experiments and Simulation, Circulation Research, 1990, **67**:826-834.
17. Pries, A.R., Neuhaus, D. and Gaehtgens, P. : Blood Viscosity in Tube Flow : Dependence on Diameter and Heamatocrit, American Journal of Physiology, 1992, **263**:H1770-H1778.
18. Pries, A.R., Secomb, T.W., Gessner, T., Sperandio, M.B., Gross, J.F. and Gaehtgens, P. : Resistance to Blood Flow in Microvessels in vivo, Circulation Research, 1994, **75**:904-915.